



New Evidence for the Mechanism of Action of a Type-2 Diabetes Drug Using a Magnetic Bead-Based Automated Biosensing Platform

Uddin, Rokon; Nur-E-Habiba; Rena, Graham; Hwu, En Te; Boisen, Anja

Published in:
ACS Sensors

Link to article, DOI:
[10.1021/acssensors.7b00384](https://doi.org/10.1021/acssensors.7b00384)

Publication date:
2017

Document Version
Peer reviewed version

[Link back to DTU Orbit](#)

Citation (APA):

Uddin, R., Nur-E-Habiba, Rena, G., Hwu, E. T., & Boisen, A. (2017). New Evidence for the Mechanism of Action of a Type-2 Diabetes Drug Using a Magnetic Bead-Based Automated Biosensing Platform. *ACS Sensors*, 2(9), 1329–1336. <https://doi.org/10.1021/acssensors.7b00384>

General rights

Copyright and moral rights for the publications made accessible in the public portal are retained by the authors and/or other copyright owners and it is a condition of accessing publications that users recognise and abide by the legal requirements associated with these rights.

- Users may download and print one copy of any publication from the public portal for the purpose of private study or research.
- You may not further distribute the material or use it for any profit-making activity or commercial gain
- You may freely distribute the URL identifying the publication in the public portal

If you believe that this document breaches copyright please contact us providing details, and we will remove access to the work immediately and investigate your claim.

New evidence for the mechanism of action of a type-2 diabetes drug using a magnetic bead-based automated biosensing platform

Rokon Uddin^{*a}, Nur-E-Habiba^b, Graham Rena^c, En-Te Hwu^d and Anja Boisen^a

^aDepartment of Micro- and Nanotechnology, Technical University of Denmark, DTU Nanotech, Building 345 East, DK-2800 Kongens Lyngby, Denmark

^bDepartment of Chemistry and Bioengineering, Tampere University of Technology, Tampere, Finland

^cMolecular and Clinical Medicine, School of Medicine, University of Dundee, Dundee, UK

^dInstitute of Physics, Academia Sinica, Nankang, Taiwan

*Corresponding author: Rokon Uddin

Contact: Ørsted's Plads, Building 345C, 110

2800 Kgs. Lyngby, Denmark

Tel: +4545256343

Email: rokud@nanotech.dtu.dk

Abstract

The mechanism of action (MOA) of the first line type-2 diabetes drug metformin remains unclear despite its widespread usage. However, recent evidence suggests that the mitochondrial copper (Cu)-binding action of metformin may contribute towards the drug's MOA. Here, we present a novel biosensing platform for investigating the MOA of metformin using a magnetic microbead-based agglutination assay which has allowed us to demonstrate for the first time the interaction between Cu and metformin at clinically relevant low micromolar concentrations of the drug, thus suggesting a potential pathway of metformin's blood-glucose lowering action. In this assay, cysteine-functionalized magnetic beads were agglutinated in the presence of Cu due to cysteine's Cu-chelation property. Addition of clinically relevant doses of metformin resulted in disaggregation of Cu-bridged bead-clusters, whereas the effect of adding a closely-related but blood-glucose neutral drug propanediimidamide (PDI) showed completely different responses to the clusters. The entire assay was integrated in an automated microfluidics platform with an advanced optical imaging unit by which we investigated these aggregation-disaggregation phenomena in a reliable, automated and user-friendly fashion with total assay time of 17 min requiring a sample (metformin/PDI) volume of 30 µl. The marked difference of Cu-binding action between the blood-glucose lowering drug metformin and its inactive analogue PDI thus suggests that metformin's distinctive Cu-binding properties may be required for its effect on glucose homeostasis. The novel automated platform demonstrating this novel investigation thus holds the potential to be utilized for investigating significant and sensitive molecular interactions via magnetic bead-based agglutination assay.

Keywords: Biosensor, type-2 diabetes, metformin, magnetic beads, agglutination assay, optical imaging, molecular interactions

415 million people have diabetes worldwide and by 2040, the number will rise to 642 million according to the latest estimates of the International Diabetes Federation (IDF); where at least 90% of these patients have type-2 diabetes. Metformin was first used in humans as a type-2 diabetes (T2D) drug in the late 1950s^{1,2} and is the first-line oral treatment for T2D. As it was discovered before the modern day target-based drug discovery era, its mechanism of

action at the molecular level was not established before its clinical use and still remains unclear today ^{1,3,4}. A detailed understanding of its molecular mechanism might lead to the development of next generation target-based drug for treating T2D. Regarding the molecular mechanism of metformin, studies have shown that treatment of liver cells with metformin leads to reduced mitochondrial respiration ⁵⁻⁸ and concomitant reduction of hepatic energy through depletion of intracellular ATP content ⁹. Thus, due to lower hepatic energy lower amount of glucose is produced by hepatic cells. However, the pathway through which metformin reduces the mitochondrial respiration is not established yet and an area of vigorous research.

This drug has been proven to interact with different metals ¹⁰⁻¹⁴ and the most stable of these interactions is with the metal copper (Cu) ^{15,16}. Recently the relationship of Cu-binding to the clinical action of metformin has been under investigation ¹⁶⁻¹⁸. The studies found that metformin binds with mitochondrial Cu under conditions where it inhibits mitochondrial respiration. Both Cu²⁺ and Cu¹⁺ ions are important ions in electron transport chain enzymes during ATP production ¹⁹⁻²¹, and inhibition of these enzymes will reduce the content of intracellular ATP, resulting in less glucose production due to lower hepatic energy ⁷. Up to now however, the cell studies with metformin, including those described above, have depended on high (1-2 millimolar or more) concentrations of drug and therefore it is unclear if they are related to lowering of the glucose level in blood (anti-hyperglycemia), which are mediated by low micromolar plasma concentrations of the drug in plasma. Consequently, in the current study we have developed tools to measure metformin's metal-binding properties at therapeutically-relevant concentrations.

Magnetic bead-based assays are being utilized for different applications like detection of small molecules ^{22,23}, pathogens ²⁴ and proteins ^{25,26}, as well as PCR amplification ²⁷ and drug delivery ^{28,29}. Detection of biomarkers or molecules by agglutination-based sensing using magnetic beads are being used for their readout simplicity ³⁰⁻³⁴. Hence, in our previous preliminary study ¹⁷, the concept of our well-studied magnetic bead-based agglutination assay ^{22,31,32,34,35} had been utilized for investigating the effects of metformin on Cu ions as a step towards understanding the mechanism of metformin. As Cu ions hardly remain as free ions in the cells ³⁶⁻³⁸ and approximately 35% of them remain bound to cysteine residues ^{39,40}, we prepared Cu-L-cysteine compound/aggregates using nano-sized magnetic beads to mimic at least 35% of Cu-ligands of the cell as these magnetic nanobead (MNB) aggregates will model particularly well protein-bound copper ions. Addition of different concentrations of metformin caused dissolution of the aggregates indicating breakage of the Cu-L-cysteine bonds. The detection of the aggregation-disaggregation phenomena was performed by a Blu-ray-based optomagnetic system ^{32,34} where the signal peaks were sensitive to the size and concentration of the aggregates. Thus, the previous agglutination assay demonstrated that metformin interacts with cysteine-bound Cu-ligand. A significant drawback however, is that it was insufficiently sensitive to study this property at physiological concentrations (micromolar) of the drug. In addition, it did not demonstrate the evidence of relationship between the Cu-binding action and its glucose lowering property.

In this paper, we present an integrated and automated biosensing platform with a substantial improvement in sensitivity compared to our previous work while using micro-sized magnetic beads (hereafter acronymed as 'MB'). These improvements have allowed us to quantify, for the first time, the effects of micromolar concentrations of metformin on copper-bridged cysteine MB aggregates. To investigate how well metformin's Cu-binding action corresponds with its glucose lowering property, we have compared the Cu-metformin interactions with an inactive analogue of the drug propanediimidamide (PDI). Although structurally similar to metformin, PDI does not show anti-hyperglycemic behavior in cells ^{16,17} nor does it exhibit anti-inflammatory effects noted recently for metformin ⁴⁰. The completely different behavior of PDI compared to metformin suggests that metformin's Cu-binding action may be required for its glucose-lowering effect. The overall study has been performed with control experiments to demonstrate the specificity of metformin's interaction with Cu-bridged MBs. Furthermore, the experimental setup has been improved compared to our previous study ¹⁸ by integrating an automated optical imaging unit (oCelloScope, Philips Biocell) for automated operation of the entire study, allowing rapid optimization of the Cu-MB clusters. The usage of micro-scale beads aided visualization and the characterization of the clusters using the imaging unit assisted in the process of the optimization of the assay protocol. The developed sensing platform has the potential to be an out-of-lab setting for studying molecular interactions through MB-based agglutination assay.

Experimental

Materials and chemicals

The MBs (Dynabeads MyOne Streptavidin T1, 10mg/ml) with a surface-coating of streptavidin used in this study were bought from Life Technologies (Thermo Scientific). EZ-Link NHS-LC-LC Biotin was ordered from VWR (Thermo Scientific, Product no. 21343) and L-cysteine was purchased from Merck KGaA (Germany). 50mM PBS (pH 7.4) and 50mM MES (pH 6.0) buffer were prepared using MilliQ water for washing and sample preparation. The drug vehicle MES buffer was prepared by dissolving 0.488 g MES hydrate (Sigma Aldrich, product no. M8250; 2-(N-Morpholino) ethanesulfonic acid) in 45 ml MilliQ water while the pH was adjusted with 1M NaOH. $\text{Cu}(\text{NO}_3)_2$ purchased from Sigma-Aldrich was prepared as 0.5mM solution in MES buffer for performing experiments. Metformin (1,1 Dimethylbiguanide hydrochloride) and PDI (Propanediimidamide dihydrochloride) purchased from Sigma-Aldrich were prepared at different concentration in MES buffer.

Sample preparation

A solution of 10mM biotin and a solution of 0.6M L-cysteine were prepared using PBS buffer (pH: 7.4). Next, the solutions of biotin and L-cysteine were mixed with a volume ratio of 1:8.5 involving 30 min incubation at room temperature (RT) for biotinylating the L-cysteine. Next, 10mg/ml micro-sized MBs (bead diameter: 1 μm) coated with streptavidin was washed three times with PBS buffer (pH: 7.4). After that, the MB solution, biotinylated L-cysteine solution and PBS buffer were mixed with a volume ratio of 1:3.5:5.5 followed by incubation of 1 hour with gentle shaking on a shaker at RT. Finally, the incubated solution was washed three times with 50mM MES buffer and resuspended at a bead concentration of 1 mg/ml.

The Biosensing Platform

In our previous study¹⁸, we used a microfluidic disc-based optomagnetic unit for demonstrating the effects of different concentrations of metformin on the clusters formed through Cu and magnetic nanobeads (MNB). In the current study, we have integrated an optical imaging unit^{34,42} onto the disc-based optomagnetic unit in order to integrate visualization and quantification of the effects of metformin on the micro-sized Cu-MB clusters (Fig. 1). The setup, in addition, facilitates the integration and automation of fluidics operation along with automated detection in a user-friendly fashion.

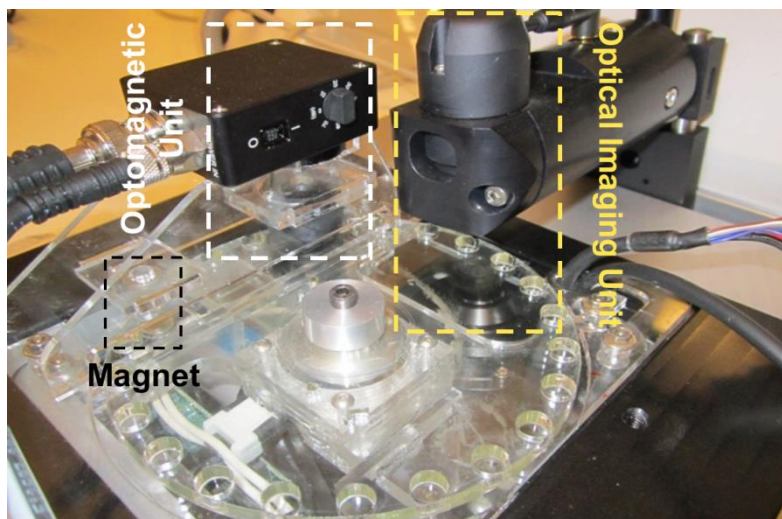


Fig. 1. Integrated platform for studying molecular interactions

Integrated experimental setup consisting of a Blu-ray based optomagnetic unit, an automated optical imaging unit and a pair of permanent magnets on a centrifugal microfluidics platform. Details of the detection units can be found in ⁴³.

The current setup (Fig. 1) consists of a removable microfluidic disc, a pair of permanent magnets mounted onto the platform for performing magnetic incubation (MI); and an optomagnetic unit along with an optical imaging unit for visualization and quantification of nano/micro particles. The disc is attached to a closed-loop motor (Maxxon Motor, mod. 273756, Switzerland) and controlled using a LabVIEW (National Instruments) based program which facilitates automation of the assay and reproducible positioning of the sample. The optical imaging unit can be moved along both the horizontal and vertical axes using the instrumental software (Uniexplorer 6.0) which facilitates automated scanning at the precise positions of the sample/disc ensuring reproducibility for multiple measurements. The automated scanning creates multiple stacks of images using optical sectioning principle of confocal microscopy resulting-in capturing all the MBs/MB-clusters in focus within the scanning window. Using the instrumental image processing algorithm, the software calculates the size i.e. the projected area of each MBs/MB aggregates and thus, gives the mean MB aggregate size in a sample. Further details of the scanning principle can be found in ^{34,42}.

Experimental procedure

The assay platform in this study was a microfluidic disc made from two layers of Polymethylmethacrylate (PMMA) and bonded by a layer of pressure sensitive adhesive (PSA). The disc (thickness 4.7 mm) contains 24 wells each of which is 4 mm in depth and 7 mm in diameter (Fig. 2a). Thus, 24 individual experiments can be performed in a single disc the fabrication of time of which is <10 min. Further information on the disc fabrication is presented in the Supplementary Material Section S1.

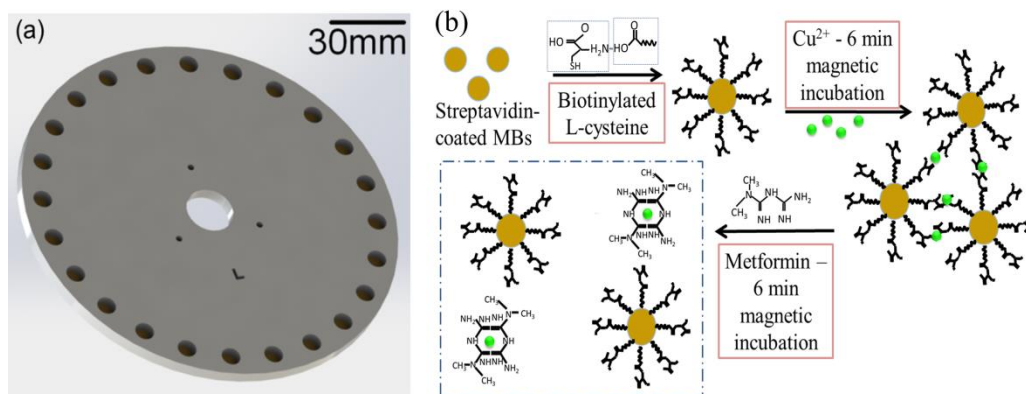


Fig. 2. Schematic of Disc and Assay Design

(a) Schematic of the microfluidic disc consisting of 24 wells where the agglutination assay is performed (b) Schematic of the agglutination assay. The MBs functionalized with biotinylated L-cysteine forms clusters through L-cysteine-Cu bond after the addition of Cu^{2+} followed by magnetic incubation, which are again disaggregated after adding metformin followed by 2nd magnetic incubation. Further information on the assay scheme is presented in the Supplementary Material Section S2.

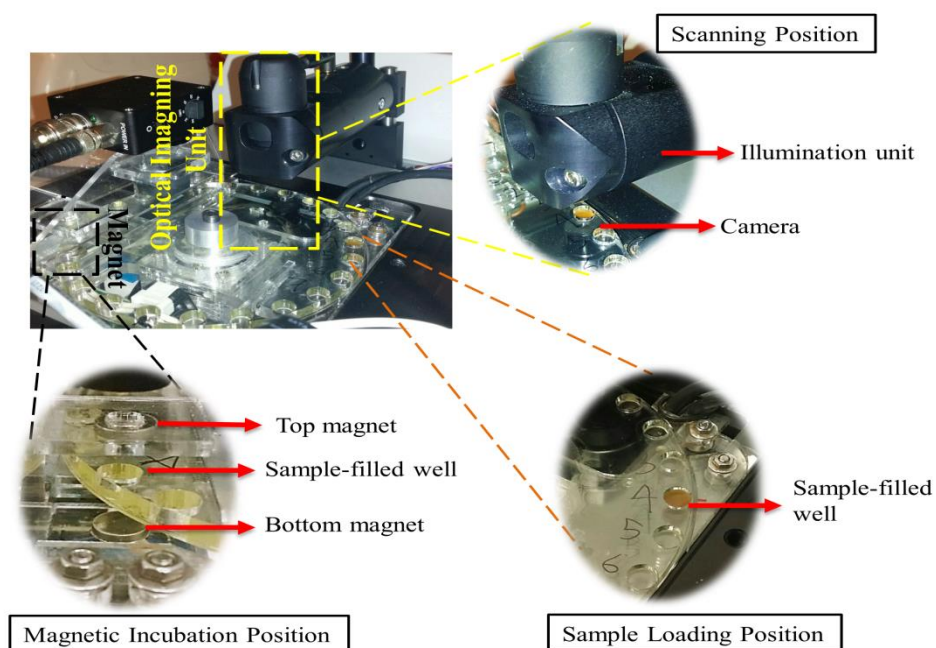


Fig 3. Detailed illustration of different significant positions of the experimental setup

The experimental setup has three defined positions: sample-loading position, magnetic incubation (MI) position and scanning position (Fig. 3). Firstly, the microfluidic disc was mounted onto the experimental setup and the well of the disc in which the Cu-MB sample was to be loaded was placed at the sample-loading position. Then, a mixed solution of Cu and streptavidin-coated MBs functionalized with biotinylated L-cysteine (volume ratio 11:1) was loaded into the particular well of the disc (Fig. 2b). After sample loading, the disc rotated following a rotation-routine set by the Labview program till the sample-filled well reached the position between the two permanent magnets (MI position) for performing MI for 6 min with a magnetic field of 60 mT. The MI protocol consisted of constant incubation (10 s) under the magnet for enhancing agglutination, followed by clockwise and anti-clockwise shaking of the disc with a speed of 30 rpm for breaking unspecific binding as well as facilitating interaction between MBs and Cu. Due to the Cu-chelation property of L-cysteine, the MBs functionalized with L-cysteine bridge with Cu through Cu-L-cysteine bond

and thus, causes the formation of Cu-MB clusters (Fig. 2b). The complete MI protocol was run by the rotation-routine made in the Labview program facilitating reproducibility of the incubation. After the completion of MI, the disc rotated following the rotation-routine for the sample-filled well to reach the precise position (scanning position) between the light source and camera of the optical imaging unit in order to perform scanning of the clusters. The solution was scanned and the captured images were analyzed by Uniexplorer 6.0 to quantify the Cu-MB clusters. After scanning, the sample-filled well was again positioned to the sample-loading position using the software in order to add 30 μ l of different concentration of metformin/PDI into the Cu-MB clusters (volume ratio 1:2). After adding the sample, the same rotation-routine was initiated to perform MI followed by scanning to quantify the clusters. The purpose of the 2nd MI was to further ensure the agglutination as well as facilitating interaction between Cu-MB clusters and metformin/PDI while breaking the non-specific bindings. The total assay time including incubation and scanning was approximately 17 min.

Results and Discussion

Interaction of metformin and PDI with copper

Our previous study using MNBs and the optomagnetic unit of the experimental setup¹⁸ showed that Cu-MNB clusters formed after addition of Cu into the MNB solution, and as millimolar concentrations of metformin were added, the Cu-MNB clusters were disaggregated accordingly.

In our current study, we were able to test millimolar and micromolar doses of metformin due to the optimization of the assay protocol and the integration of the imaging unit. In the first experiment, we investigated the effect of higher doses (0.5-50mM) of metformin on Cu-MB disaggregation (Fig. 4). We found that at each concentration tested, metformin disaggregated the beads.

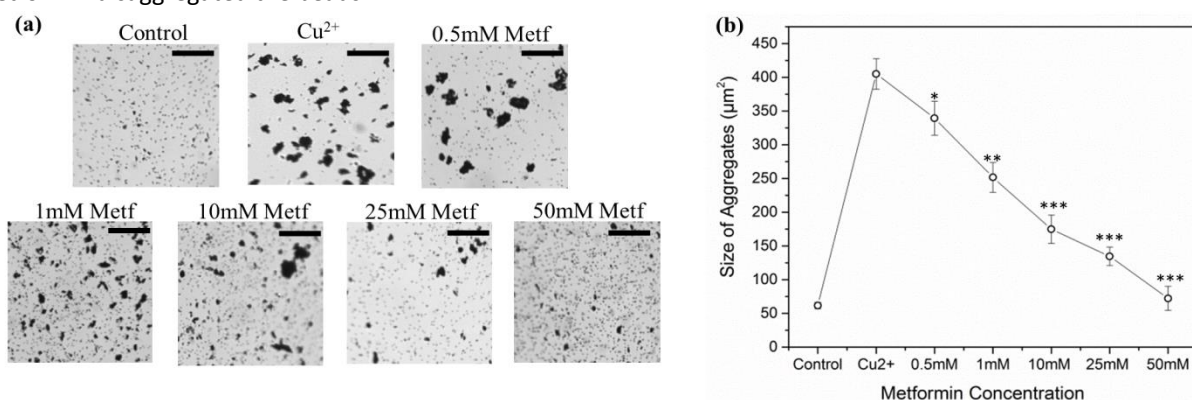


Fig. 4: Effect of adding metformin (Metf) at different concentrations into the Cu-MB clusters.

(a) Images captured by the optical imaging unit of different MB samples. (b) Corresponding mean area of MB aggregates (calculated by Uniexplorer 6.0) vs. different MB samples. Error bars indicate the standard deviation obtained from triplicate measurements. Scale bar: 50 μ m. * $P < 0.05$, ** $P < 0.01$, *** $P < 0.001$ by one way ANOVA test comparing to Cu²⁺ sample.

The control/blank sample containing only MBs suspended in MES buffer shows no MB clusters (Fig. 4). Addition of Cu²⁺ into the control sample followed by 1st MI forms the Cu-MB clusters. This aggregation phenomena indicates that addition of Cu²⁺ along with MI causes the L-cysteine-functionalized MBs to bind to Cu²⁺ through the formation of Cu-L-cysteine bond. Then, the addition of different concentrations of metformin into the Cu²⁺ sample followed by 2nd MI causes the breakage of the clusters. As the MBs were aggregated based on the Cu-L-cysteine bond, this disaggregation phenomena indicates that metformin has caused the breakage of Cu-L-cysteine bond.

Next, we investigated the effect of the same concentrations of PDI on the Cu-MB clusters, to compare with that of metformin (Fig. 5). We found that addition of PDI did not reduce the Cu-MB clusters at lower concentrations and from 10 mM onwards, PDI increased the size of the clusters. These results demonstrate that PDI does not break the Cu-L-cysteine bond like metformin. Although they are structurally similar to metformin, malonamides like PDI are not anti-hyperglycaemic⁴⁴ and thus, these results are consistent there being a link between the metformin's Cu-binding action and its anti-hyperglycaemic properties.

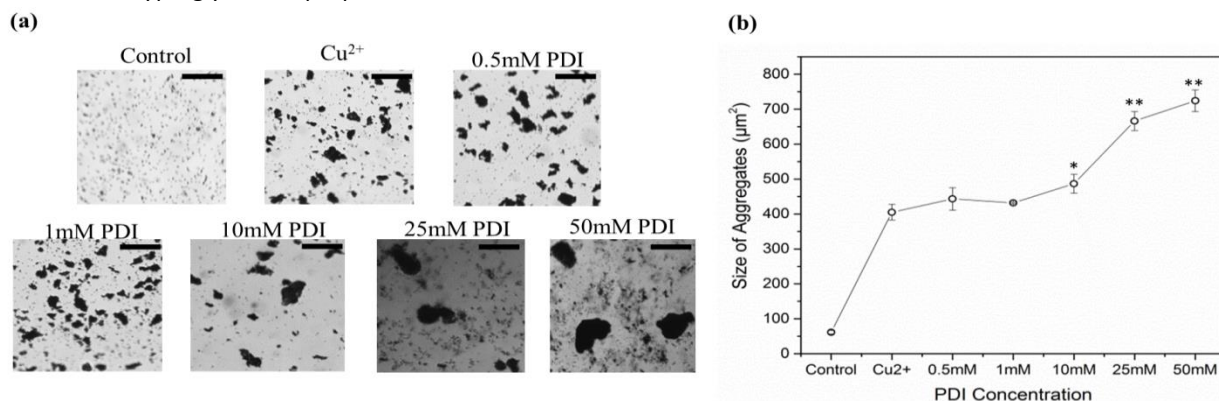


Fig. 5: Effect of adding PDI at different concentrations into the MB-Cu clusters.

(a) Images captured by the optical imaging unit of different MB samples. (b) Corresponding mean area of MB aggregates (calculated by Uniexplorer 6.0) vs. different MB samples. Error bars indicate that the standard deviation obtained from triplicate measurements. Scale bar: 50µm. *P<0.05, **P<0.01 by one way ANOVA test comparing to Cu²⁺ sample.

Control experiments

We performed control experiments in order to validate that we had measured true effects of metformin and PDI and their interaction with copper ions. In order to validate that it is not MI but Cu which forms the aggregates, a sample containing MES (copper vehicle) and functionalized MBs with a volume ratio of 11:1 (similar ratio to the Cu-MB sample) was loaded into the disc followed by 1st MI which showed no clusters (Fig. 6a). Then, MES buffer alone was further added to this solution followed by 2nd MI to mimic the addition of metformin/PDI into Cu-MB solution. Even after the 2nd MI, no significant clusters were formed which shows that it is Cu and not MI, which causes the larger clusters to form (Fig. 6a, 6b).

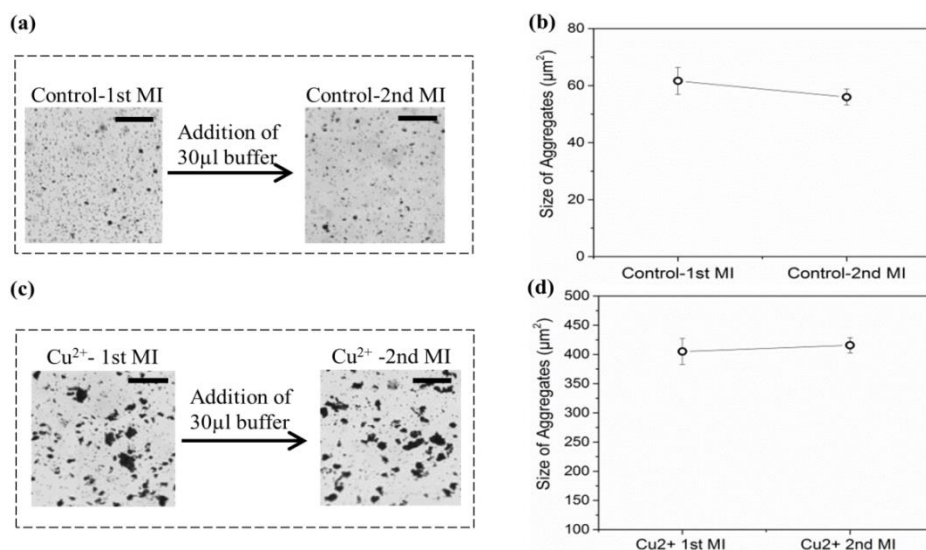


Fig. 6: Control experiments to validate that the assay is measuring drug/metal interactions

(a) Images captured by the optical imaging unit showing a comparison of the MB aggregate size between the 1st and 2nd MI of the control sample after adding 30µl of buffer (b) Corresponding mean area of MB aggregates (calculated by Uniexplorer 6.0) vs. the control samples. (c) Images captured by the optical imaging unit showing a comparison of the Cu-MB aggregate size between the 1st and 2nd MI of Cu²⁺ samples. (d) Corresponding mean area of MB aggregates (calculated by Uniexplorer 6.0) vs. the Cu²⁺ samples. Error bars indicate the standard deviation obtained from triplicate measurements. Scale bar: 50µm.

To validate the effect of metformin/PDI on Cu-MB clusters, we added 30µl of MES (drug vehicle) in the Cu-MB clusters followed by 2nd MI which showed no significant change in cluster size (Fig. 6c, 6d). This vehicle control strongly indicates that the effects of metformin and PDI are true drug-dependent effects. Together, these results indicate that Cu is required to form the large-scale aggregates and that metformin alone disaggregates these beads.

Assay optimization to detect metformin/copper interaction at physiological drug concentrations

The peak plasma concentration of metformin is in the region of 25-50 micromolar⁴⁵ and consequently we were interested in investigating the metformin/Cu interactions at these lower concentrations. In order to optimize the assay sensitivity to lower concentrations of metformin, we focused on the volume ratio of biotin and L-cysteine during the sample preparation step because the biotinylated L-cysteine is a significant component of this assay as it functions as a linker between Cu and streptavidin-coated MBs to enable aggregation. The initial volume ratio of biotin and L-cysteine was 1:8.5 by which the millimolar effects of metformin have been demonstrated above. At this volume ratio, we noted the presence of free MBs as well as heterogenous MB clusters of smaller and larger size (Fig. 7a) indicating that many of MBs were not sufficiently functionalized with L-cysteine, due to insufficient biotinylation of L-cysteine. Probably because of this heterogeneity, we were unable to reliably detect effects of low concentrations of metformin on these MB aggregates. To improve sensitivity, we hypothesized that there might be an optimal ratio of biotin: L-cysteine, where most of the MBs would be homogeneously functionalized with biotinylated L-cysteine, leading to the formation of Cu-MB clusters of increased homogeneity and potentially improve assay sensitivity. Optimizing MB functionalization with L-cysteine through maximizing the biotinylation of L-cysteine would increase the probability of MBs agglutinating more specifically through Cu bridges, potentially increasing the sensitivity of the assay to metformin-induced disaggregation. We varied the biotin: L-cysteine ratio in two stock solutions from 1:8.5 (highC sample) to 1:4.5 (lowC sample) and 1:2.5 (very lowC sample) by increasing the volume of biotin. The amount of L-cysteine was kept constant as reducing cysteine further below would ultimately result in a failure of aggregates to

form. We compared side by side the Cu-MB clusters formed from MB samples with these three different biotin and L-cysteine ratios (Fig. 7a) and found indeed that the lowC ratio formed aggregates that were much more homogenous in size and densely packed than in the highC sample.

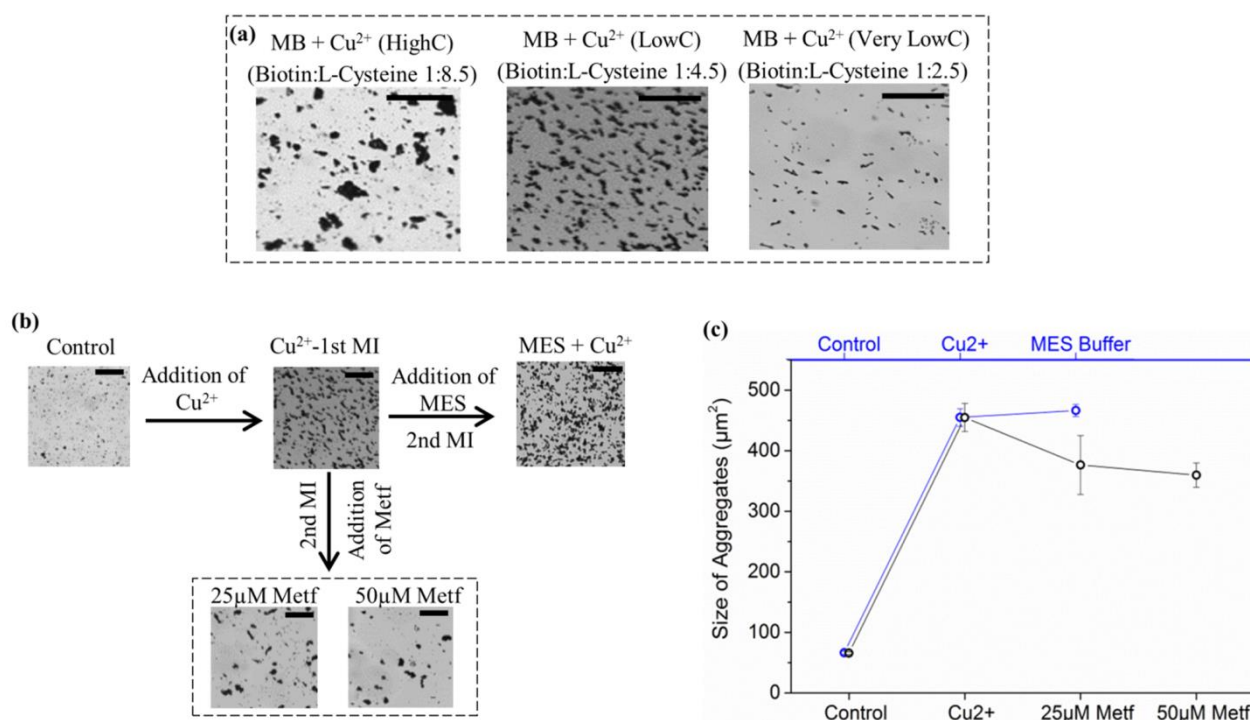


Fig. 7. High sensitivity assay measures metformin/Cu interaction at physiological concentrations of the drug.

(a) Images captured by the optical imaging unit showing a comparison of Cu-MB clusters of the samples with different biotin-L-cysteine ratios. (b) Effect of low concentrations of metformin (Metf) on Cu-MB clusters using the lowC sample. Images captured by the optical imaging unit showing the effects of adding metformin at different concentrations at micromolar range into the Cu-MB clusters. (c) Mean MB aggregates size (calculated by Uniexplorer 6.0) vs. different MB samples. The blue line indicates the result of the control experiment which shows that addition of Cu²⁺ into control/blank sample creates Cu-MB clusters followed by addition of MES showing no significant change. Error bars indicate the standard deviation obtained from triplicate measurements. Scale bar: 50μm. *P<0.05 by one way ANOVA test comparing to MES+Cu²⁺ sample.

Compared to both of these samples, the very low C sample, which was prepared by adding a much higher volume of biotin, resulted in Cu-MB clusters much smaller both in size and in amount, confirming that saturation with biotin eventually blocks aggregate formation, likely because the excess amount of free biotin saturated the binding sites of streptavidin on the MBs.

We used the improved formulation of the lowC sample to study the effects of metformin at low concentrations (Fig. 7b and 7c). As before, the addition of Cu²⁺ into the MB solution followed by MI resulted in clusters. Further addition of 25μM or 50μM metformin followed by 2nd MI causes the breakage of the clusters indicating that metformin does interact with Cu²⁺ from the Cu-L-cysteine bond, even at micromolar concentrations. To validate this experiment, MES buffer (instead of metformin) was added to Cu-MB solution followed by MI, which showed again no significant change to the clusters.

We thus found that the formulation of the lowC sample was a crucial development to enable visualizing the effect of metformin in the micromolar range. In future work, we will continue to pursue further possibilities for optimization in order to make the assay more sensitive and robust.

Conclusion and Future work

We have developed an improved experimental set-up to study molecular interactions using magnetic bead-based agglutination assay. Using this equipment along with the optimized assay, we demonstrate for the first time that metformin interacts with copper ions at physiologically significant concentrations of the drug. Furthermore, our experiments comparing the effects of metformin and PDI strongly suggest that metformin's Cu-binding property may be linked to its therapeutic drug action. These results create a platform for future work to further investigate the effects of metformin directly in blood cells and hepatic cells at μM concentrations by adaptation of the magnetic bead-based agglutination assay we have developed. However, utilization of magnetic bead-based agglutination assay in raw biological samples (e.g. plasma or cells) is challenging as endogenous interferents can form unspecific magnetic bead clusters decreasing the specificity and sensitivity of the assay. Therefore, in our next study with raw biological samples, we will integrate the biotin-L-cysteine conjugation protocol with our previously presented³⁰ anti-fouling surface architecture development through the formation of a layer of blocking proteins on the bead surface in order to prevent non-specific aggregate formation under the influence of the biological samples. As serum albumin is well-known to minimize protein aggregation⁴⁶, likewise in a previous study³¹, the surface of the MBs firstly would be passivated with a monolayer of human serum albumin (HSA) for preventing the formation of undesired protein corona in plasma samples. The HSA monolayer on the MB surface would be attached to L-cysteine through biotinylated biorthogonal click conjugation (e.g. Cu-free click chemistry) forming a multi-layered surface structure over MB surface for such surface structures previously demonstrated dramatic increase of assay sensitivity as well as facilitation of specific cross-linking of the affinity probes in biological fluids^{31,47}. The entire assay can be integrated in the microfluidic disc with additional microfluidic structures for on-disc plasma extraction from whole blood sample. For cellular studies, a fluorescence probe can be added to the MBs with multi-layered surface architecture followed by microinjecting the conjugate in hepatic (e.g. H4IIE) cells. Thus, the presence of cellular Cu-L-cysteine is expected to form Cu-bridged MB clusters inside the cells while quenching the fluorescence. Adding metformin to the cell medium and its uptake into the cell will be expected to cause disintegration of the aggregates while restoring the fluorescence. Hence, the extension of this study in future can be performed in raw biological samples by overcoming the potential challenges of biological interferences and thus adding further validation to this current study of metformin's Cu-binding action at cellular concentrations. In conclusion, the developed biosensing platform demonstrating automation, low sample-to-answer time along with a novel application, thus paves the way for investigating further significant molecular interactions using the simple readout concept of agglutination assay in a reliable and user-friendly fashion.

Supporting Information

Supporting Information Available: The following files are available free of charge.

Supplementary information.pdf

- Description of the disc fabrication process and the detailed chemical bonding schematics of the assay

Acknowledgements

This work was financially supported by the European Research Council under the European Union's Seventh Framework Program (FP7/2007-2013) grant no. 320535-HERMES. The authors also acknowledge the support from the IDUN project (grant no. DNR122) funded by the Danish National Research Foundation and the Velux Foundations. G. Rena acknowledges funding from MRC (MR/K012924/1).

References

1. Rena G, Pearson ER, Sakamoto K. Molecular mechanism of action of metformin: Old or new insights? *Diabetologia*. 2013;56(9):1898–906.
2. Rojas LBA, Gomes MB. Metformin: an old but still the best treatment for type 2 diabetes. *Diabetol Metab Syndr*. 2013;5(1):6.
3. Viollet B, Guigas B, Sanz Garcia N, Leclerc J, Foretz M, Andreelli F. Cellular and molecular mechanisms of metformin: an overview. *Clin Sci (Lond)*. 2012;122(6):253–70.
4. Rena G, Pearson ER, Hardie DGH. The mechanisms of action of metformin. *Diabetologia*. 2017 (In Press), DOI: 10.1007/s00125-017-4342-z.
5. Owen MR, Doran E, Halestrap AP. Evidence that metformin exerts its anti-diabetic effects through inhibition of complex 1 of the mitochondrial respiratory chain. 2000;614:607–14.
6. El-Mir MY, Nogueira V, Fontaine E, Avéret N, Riquelme M, Leverve X. Dimethylbiguanide Inhibits Cell Respiration via an Indirect Effect Targeted on the Respiratory Chain Complex I. *J Biol Chem*. 2000;275:223–8.
7. Foretz M, Hébrard S, Leclerc J, Zarrinpashneh E, Soty M, Mithieux G, Sakamoto K, Andreelli F, Viollet B. Metformin inhibits hepatic gluconeogenesis in mice independently of the LKB1/AMPK pathway via a decrease in hepatic energy state. *J Clin Invest*. 2010;120(7):2355–69.
8. Madiraju AK, Erion DM, Rahimi Y, Zhang XM, Braddock DT, Albright RA, Prigaro BJ, Wood JL, Bhanot S, MacDonald MJ, Jurczak MJ, Camporez JP, Lee HY, Cline GW, Samuel VT, Kibbey RG, Shulman GI. Metformin suppresses gluconeogenesis by inhibiting mitochondrial glycerophosphate dehydrogenase. *Nature*. 2014;510(7506):542–6.
9. Foretz M, Guigas B, Bertrand L, Pollak M, Viollet B. Metformin: From mechanisms of action to therapies. *Cell Metab*. 2014;20(6):953–66.
10. Ray RK KG. Metal and Non-Metal Biguanide Complexes. New Delhi: New Age International Publishers; 1999.
11. Ray RK KG. An EPR study of Copper (II)-substituted Biguanide Complexes. Part III. *Inorg Chim Acta*. 1990;174:237–44.
12. Zhu M, Lu L, Yang P JX. Bis, (1,1-dimethylbiguanido)copper(II) octahydrate. *Acta Crystallogr Sect E*. 2002;58:217–9.
13. Gholivand MB, Mohammadi-Behzad L. Differential pulse voltammetric determination of metformin using copper-loaded activated charcoal modified electrode. *Anal Biochem*. 2013;438(1):53–60.
14. Sharma SS, Ramani JV, Dalwadi DP, Bhalodia JJ, Patel NK, Patel DD, Patel RK. New Ternary Transition Metal Complexes of 2-[[[(2-aminophenyl)imino] methyl]Phenol and Metformin: Synthesis, Characterization and Antimicrobial Activity. *EJ Chem*. 2011;8(1):361–7.
15. Ray P. Complex Compounds of Biguanides and Guanyureas With Metallic Element. *Chem Rev*. 1961;61(4):313–59.
16. Logie L, Harthill J, Patel K, Bacon S, Hamilton DL, Macrae K, McDougal G, Wang HH, Xue L, Jiang H, Sakamoto K, Prescott AR, Rena G. Cellular responses to the metal-binding properties of metformin. *Diabetes*. 2012;61(6):1423–33.
17. Repiščák P, Erhardt S, Rena G, Paterson MJ. Biomolecular mode of action of metformin in relation to its copper binding properties. *Biochemistry*. 2014;53(4):787–95.
18. Quan X, Uddin R, Heiskanen A, Parmvi M, Nilson K, Donolato M, Hansen MF, Rena G, Boisen A. The copper binding properties of metformin - QCM-D, XPS and nanobead agglomeration. *Chem Commun*. 2015;51(97):17313–6.
19. Lodish H, Berk A, Zipursky SL, Matsudaira P, Baltimore D, Darnell J. Electron Transport and Oxidative Phosphorylation. In: *Molecular Cell Biology* 4th edition. New York: W.H. Freeman; 2000. Section 16.2.
20. Banci L, Bertini I, Cantini F, Ciofi-Baffoni S. Cellular copper distribution: A mechanistic systems biology approach. *Cell Mol Life Sci*. 2010;67(15):2563–89.
21. Horn D, Barrientos A. Mitochondrial copper metabolism and delivery to cytochrome C oxidase. *IUBMB Life*. 2008;60(7):421–9.
22. Yang J, Donolato M, Pinto A, Bosco FG, Hwu ET, Chen CH, Alstrøm TS, Lee GH, Schäfer T, Vavassori P, Boisen A, Lin Q, Hansen MF. Blu-ray based optomagnetic aptasensor for detection of small molecules. *Biosens Bioelectron*. 2016;75:396–403.
23. Wu S, Duan N, Wang Z, Wang H. Aptamer-functionalized magnetic nanoparticle-based bioassay for the detection of ochratoxin A using upconversion nanoparticles as labels. *Analyst*. 2011;136(11):2306–14.
24. El-Boubbou K, Gruden C, Huang X. Magnetic glyco-nanoparticles: A unique tool for rapid pathogen detection, decontamination, and strain differentiation. *J Am Chem Soc*. 2007;129(44):13392–3.
25. Horng HE, Yang SY, Hong CY, Liu CM, Tsai PS, Yang HC, Wu CC. Biofunctionalized magnetic nanoparticles for high-sensitivity immunomagnetic detection of human C-reactive protein. *Appl Phys Lett*. 2006;88(25):252506.
26. Tsai HY, Hsu CF, Chiu IW, Fuh CB. Detection of C-reactive protein based on immunoassay using antibody-conjugated

- magnetic nanoparticles. *Anal Chem.* 2007;79(21):8416–9.
27. Kojima T, Takei Y, Ohtsuka M, Kawarasaki Y, Yamane T, Nakano H. PCR amplification from single DNA molecules on magnetic beads in emulsion: Application for high-throughput screening of transcription factor targets. *Nucleic Acids Res.* 2005;33(17):1–9.
 28. Wilson KS, Goff JD, Riffle JS, Harris LA, St Pierre TG. Polydimethylsiloxane-magnetite nanoparticle complexes and dispersions in polysiloxane carrier fluids. *Polym Adv Technol.* 2005;16(2–3):200–11.
 29. Jain TK, Richey J, Strand M, Leslie-Pelecky DL, Flask CA, Labhasetwar V. Magnetic nanoparticles with dual functional properties: Drug delivery and magnetic resonance imaging. *Biomaterials.* 2008;29(29):4012–21.
 30. Ranzoni A, Sabatte G, van Ijendoorn LJ, Prins MWJ. One-step homogeneous magnetic nanoparticle immunoassay for biomarker detection directly in blood plasma. *ACS Nano.* 2012;6(4):3134–41.
 31. Antunes P, Watterson D, Parmvi M, Burger R, Boisen A, Young P, Copper MA, Hansen MF, Ranzoni A, Donolato M. Quantification of NS1 dengue biomarker in serum via optomagnetic nanocluster detection. *Sci Rep.* 2015;5:16145.
 32. Donolato M, Antunes P, de la Torre TZG, Hwu ET, Chen CH, Burger R, Rizzi G, Bosco FG, Strømme M, Boisen A, Hansen FM. Quantification of rolling circle amplified DNA using magnetic nanobeads and a Blu-ray optical pick-up unit. *Biosens Bioelectron.* 2015;67:649–55.
 33. Göransson J. Sensitive detection of bacterial DNA by magnetic nanoparticles. *Anal Chem.* 2010;82(22):9138–40.
 34. Uddin R, Burger R, Donolato M, Fock J, Creagh M, Hansen MF, Boisen A. Lab-on-a-disc agglutination assay for protein detection by optomagnetic readout and optical imaging using nano- and micro-sized magnetic beads. *Biosens Bioelectron.* 2016;85:351–7.
 35. Mezger A, Fock J, Antunes P, Østerberg FW, Boisen A, Nilsson M, Hansen MF, Ahlford A, Donolato M. Scalable DNA-Based Magnetic Nanoparticle Agglutination Assay for Bacterial Detection in Patient Samples. 2015;(7):7374–82.
 36. Abajian C, Yatsunyk LA, Ramirez BE, Rosenzweig AC. Yeast Cox17 solution structure and copper(I) binding. *J Biol Chem.* 2004;279(51):53584–92.
 37. Boal AK, Rosenzweig AC. Structural biology of copper trafficking. *Chem Rev.* 2009;109(10):4760–79.
 38. Rubino JT, Franz KJ. Coordination chemistry of copper proteins: How nature handles a toxic cargo for essential function. *J Inorg Biochem.* 2012;107(1):129–43.
 39. Wu Z, Fernandez-Lima FA, Russell DH. Amino acid influence on copper binding to peptides: Cysteine versus arginine. *J Am Soc Mass Spectrom.* 2010;21(4):522–33.
 40. Zheng H, Chruszcz M, Lasota P, Lebioda L, Minor W. Data mining of metal ion environments present in protein structures. *J Inorg Biochem.* 2008;102(9):1765–76.
 41. Cameron AR, Morrison VL, Levin D, Mohan M, Forteath C, Beall C, McNeilly AD, Balfour DJ, Savinko T, Wong AK, Viollet B, Sakamoto K, Fagerholm SC, Foretz M, Lang CC, Rena G. Anti-Inflammatory Effects of Metformin Irrespective of Diabetes Status. *Circ Res.* 2016;119(5):652–65.
 42. Fredborg M, Andersen KR, Jørgensen E, Droce A, Olesen T, Jensen BB, Rosenvinge FS, Sondergaard TE. Real-time optical antimicrobial susceptibility testing. *J Clin Microbiol.* 2013;51(7):2047–53.
 43. Uddin R, Burger R, Donolato M, Fock J, Creagh M, Hansen MF, Boisen A. Integration of agglutination assay for protein detection in microfluidic disc using blu-ray optical pickup unit and optical fluid scanning. In: *MicroTAS 2015 - 19th International Conference on Miniaturized Systems for Chemistry and Life Sciences.* 2015.
 44. Fanshawe WJ, Buer VJ, Ullman EF, Safir SR. Synthesis of unsymmetrically substituted malonamides. *J Org Chem.* 1964; 29(2): 308–311.
 45. Goodman & Gilman's *The Pharmacological Basis of Therapeutics*; Brunton LL, Chabner BA, Knollmann BC, Eds.; McGraw-Hill: New York, 2011.
 46. Finn TE, Nunez AC, Sunde M, Easterbrook-Smith SB. Serum albumin prevents protein aggregation and amyloid formation and retains chaperone-like activity in the presence of physiological ligands. *J Biol Chem.* 2012;287(25):21530–40.
 47. Sanjaya, K. C., Ranzoni, A., Watterson, D., Young, P. & Cooper, M. A. Evaluation of direct versus multi-layer passivation and capture chemistries for nanoparticle-based biosensor applications. *Biosens Bioelectron.* 2015; 67, 769–774.

For TOC only

